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Adaptive contrast imaging: transmit frequency optimization

Sébastien Ménigot^a, Anthony Novell^a, Iulian Voicu^a, Ayache Bouakaz^a and Jean-Marc Girault^{a*}

^aUniversité François Rabelais de Tours, Inserm U930, CNRS ERL 3106,
10 boulevard Tonnellé, F-37032 Tours, France

Introduction: Since the introduction of ultrasound (US) contrast imaging, the imaging systems use a fixed emitting frequency. However it is known that the insonified medium is time-varying and therefore an adapted time-varying excitation is expected. We suggest an adaptive imaging technique which selects the optimal transmit frequency that maximizes the acoustic contrast. Two algorithms have been proposed to find an US excitation for which the frequency was optimal with microbubbles.

Methods and Materials: Simulations were carried out for encapsulated microbubbles of 2 microns by considering the modified Rayleigh-Plesset equation for 2 MHz transmit frequency and for various pressure levels (20 kPa up to 420kPa). *In vitro* experiments were carried out using a transducer operating at 2 MHz and using a programmable waveform generator. Contrast agent was then injected into a small container filled with water.

Results and discussions: We show through simulations and *in vitro* experiments that our adaptive imaging technique gives: 1) in case of simulations, a gain of acoustic contrast which can reach 9 dB compared to the traditional technique without optimization and 2) for *in vitro* experiments, a gain which can reach 18 dB. There is a non negligible discrepancy between simulations and experiments. These differences are certainly due to the fact that our simulations do not take into account the diffraction and nonlinear propagation effects. Further optimizations are underway.

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*Corresponding author. Tel.: +33-(0)-247366221; fax: +33-(0)-247366120. E-mail address: jean-marc.girault@univ-tours.fr

1. INTRODUCTION

The US contrast imaging domain is in full effervescence. Currently the scientific community of this field seeks US excitations which should make possible the optimization of the acoustic contrast. We tackled the problem in a simple way by proposing an adaptive imaging technique which seeks the emitting frequency that maximizes the acoustic contrast. The use of an adaptive technique is justified by the fact that:

1. during the clinical examination, the insonified medium perfused by the microbubbles is a non-stationary medium (the concentration of bubbles changes...) ;
2. the pressure level is unknown because of the diffraction and attenuation effects which vary from one patient to another ;
3. the size and the distribution of the microbubbles of the contrast agent are not precisely known and can differ from one sample to another.

To overcome these problems, that is to disregard these unknown factors, it seemed more judicious to propose an US excitation whose frequency is selected in an adaptive way using the technique of the gradient ascent or the technique of the golden section search.

2. Methods and materials

2.1. Methods

The optimization aims to maximizing the energy of the backscattering signal by iterative method. The principle consists in first measuring the scattered power from the microbubbles, for a sinus wave excitation ; secondly to seek for the optimal transmit frequency by maximizing the scattered power.

To avoid the destruction of the microbubbles, the sinus wave train has been modulated with a Gaussian window (fig. 1). Moreover, the length of the pulse has been fixed to the power level was the same for every frequency.

These optimization methods of scattered signals do not need *a priori* knowledges of the microbubbles. The single constraint is that power must follow a convex curve on the interval where maximum energy is sought.

Two algorithms have been chosen to find the frequency of the truncated sinus incoming signal which maximizes the scattered power:

- golden section search [1]:

This approach has been chosen because it does not need to compute the derivative of energy. The first step consists in choosing two frequencies (f_1 and f_2) in the analyzed bandwidth and to compute respectively their energies (E_1 and E_2). From f_1 and f_2 , f_3 and f_4 and their corresponding energies E_3 and E_4 are calculated such as:

$$\begin{cases} f_3 = f_1 + \rho \cdot \Delta f \\ f_4 = f_2 - \rho \cdot \Delta f \end{cases} \quad (1)$$

where $\Delta f = f_2 - f_1$ and ρ is golden ratio. From the fourth iteration:

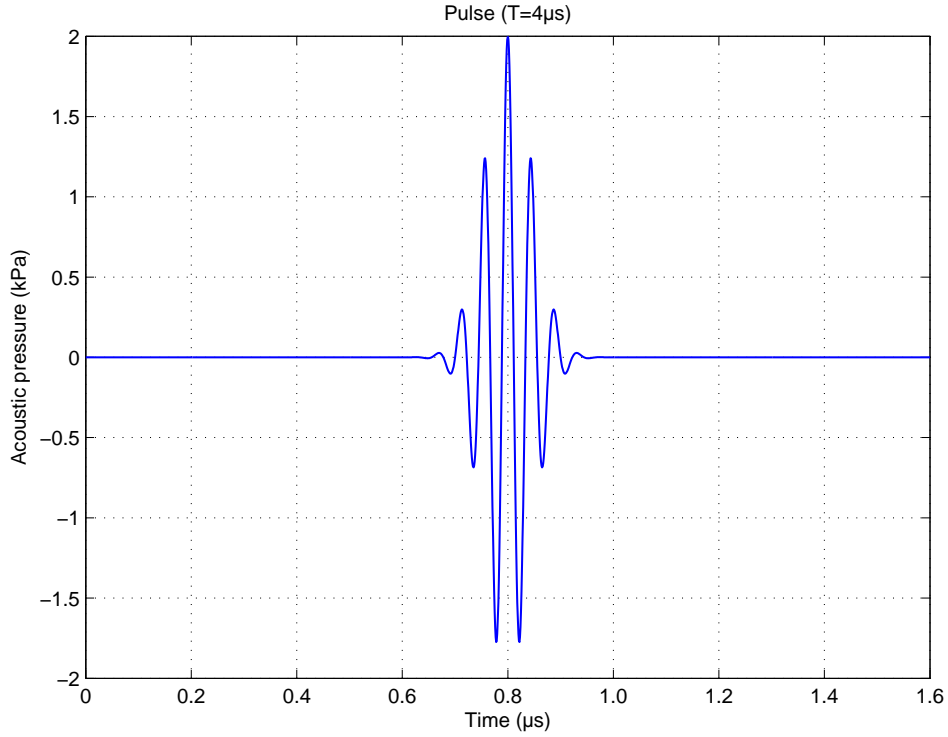


Figure 1. Emission signal

- if $E_3 > E_4$, $f_2 = f_4$, $E_2 = E_4$, $f_4 = f_3$ and $E_4 = E_3$ are assigned. A new f_3 and its energy are computed.
- if $E_4 > E_3$, $f_1 = f_3$, $E_1 = E_3$, $f_3 = f_4$ and $E_3 = E_4$ are assigned. A new f_4 and its energy are computed.
- Gradient ascent [2]:
This one maximizes energy with a recurrence relation.

$$f_{k+1} = f_k + \alpha_k \cdot \nabla E(f_k) \quad (2)$$

Note that the analytic expression of energy according to frequency is unknown. The gradient is estimated with the discrete gradient

$$\nabla E(f_k) = \frac{E_k - E_{k-1}}{f_k - f_{k-1}} \quad (3)$$

This ratio is nearly null for small energy in comparison with the frequency. The frequency is modified with a given step Δf and α_k has been chosen constant. Note that for every sign change of two successive gradients, α_k is divided by two.

2.2. Materials

2.2.1. Microbubbles

The ultrasound contrast medium was composed of SonovueTM microbubbles [3]. They have a mean size of 2.5 μm -diameter and 90% have diameters less than 10 μm . Their resonance frequency is 2.1 MHz for a 3.2 μm bubble [4].

In simulation with Bubblesim [5], the modified Rayleigh-Plesset equation (eq. 4) has been resolved with transducer effects for only one microbubble immersed in water. A microbubble of 2 μm -radius and 4 nm shell thickness has been considered.

$$\ddot{R}(t)\dot{R}(t) + \frac{3}{2}\dot{R}(t)^2 + \frac{p_0 + p_i(t) - p_L(t)}{\rho_L} - \frac{R(t)}{\rho_L c_L} \dot{p}_L(t) = 0 \quad (4)$$

with R instantaneous radius of microbubble and their derivative, p_0 static pressure, p_i instantaneous acoustic pressure, p_L liquid pressure on the surface of the microbubbles, ρ_L liquid density and c_L velocity of sound in the liquid.

Their backscattered energy has been computed with a mean energy on ten received signals to cancel out the motion of microbubbles.

2.2.2. Acoustical Measurements

Each method was compiled using Matlab[®] (Mathworks, Natick, MA) and the resulting excitation signal was transmitted through a GPIB port (National Instruments, Austin, TX) to an arbitrary function generator (33220A, Agilent, Palo Alto, CA). The signal was then amplified using a power amplifier (Amplifier Research 150A100B, Souderton, PA) and transmitted to a 1.9 MHz PZT single element (Sofranel, Sartrouville, France) focused at 55 mm and with a bandwidth of 80% (fig. 2).

Responses of a 1/2000 diluted solution of SonovueTM microbubbles (Bracco Research, Geneva, Switzerland) were measured by a 3.5 MHz PZT single element transducer with a bandwidth of 63% (fig. 3) also focused at 55 mm and used in receive mode.

Both transducers were placed perpendicularly to avoid direct transmission (fig. 4).

Measured echoes were amplified by 30 dB (Panametrics, Sofranel, Sartrouville, France) and then visualized on a digital oscilloscope (Tektronix, Beaverton, OR). Signals were finally transferred to a personal computer through a GPIB port for further analysis.

The effects of transducers have been compensated with their bandwidth by an amplitude coefficient.

To compare the adaptive technique to the traditional technique, the central frequency of emission transducers was a reference frequency.

3. Results

3.1. Simulations

To know the evolution energy according to the frequency, a microbubble has been stimulated during 4 μs and the backscattering signal has been computed for different pressures.

The frequency which allows obtaining a maximum energy varies with the pressure: for a high pressure, the frequency is lower (fig 5). From the appearance of energy, the initial frequencies for the algorithms have been chosen to find global maximum.

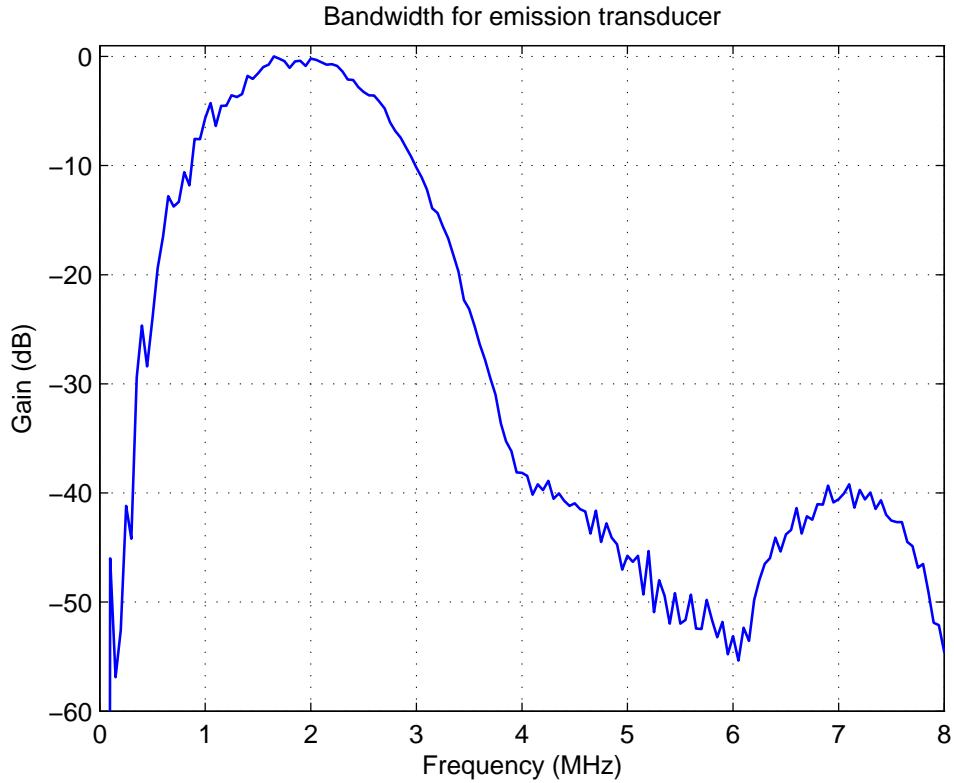


Figure 2. Bandwidth of emission transducer

The golden section search is applied with three signals of 140 kPa, 280 kPa and 480 kPa maximal pressure. The optimal frequencies permit to have a positive gain which reach 8.95 dB for a pressure of 140 kPa (fig. 6). They are stable after ten iterations. For each pressure, the optimal frequency is different (2.99 MHz, 2.69 MHz and 2.46 MHz respectively for 140 kPa, 280 kPa and 480 kPa), which the energy according to the frequency showed.

The optimization has been done again with the same signal amplitude. The gradient ascent has found the same optimal frequencies (fig 7).

3.2. Experiments

To compute the optimal frequency, a cloud of microbubbles has been stimulated during $10 \mu\text{s}$ to avoid an impulse stimulation. Three pressures (140, 280 and 420 kPa) have been applied.

For the golden section search, the optimal frequency has been found around 1.1 MHz with a gain which can reach 18 dB (fig. 8).

For the gradient ascent, the optimal frequency fluctuated between 1.3 MHz for 280 kPa and 1.1 MHz for 420 kPa (fig. 9). The gains are similar compared with the other algorithm, it is around 18 dB.

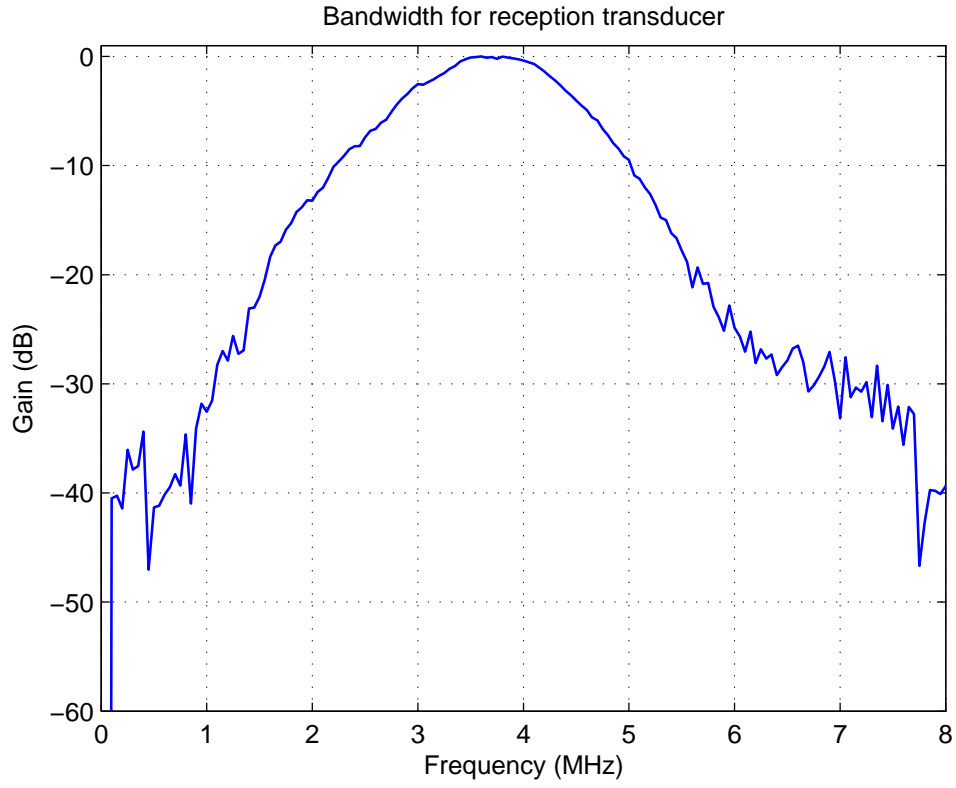


Figure 3. Bandwidth of reception transducer

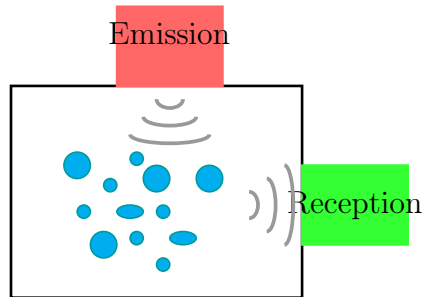


Figure 4. System

4. Discussions

These adaptive imaging techniques have allowed to:

- in case of simulations, a gain which can reach 9 dB compared to the traditional technique,

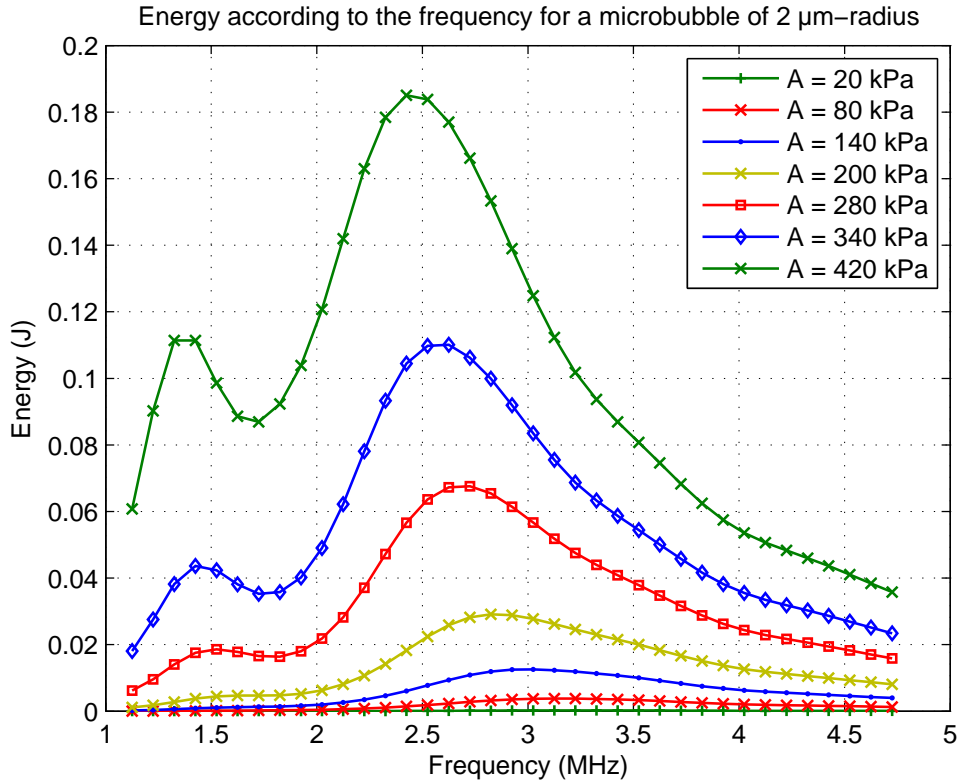


Figure 5. Energy according to frequency for a microbubble of $2 \mu m$ radius

- for *in vitro* experiments, a gain which can reach 18 dB.

According to the pressure applied to microbubbles, the optimal frequency changes. After around ten iterations, the optimal frequency has been found and the energy of the microbubbles is stable.

The experimental results are not exactly identical because of the non-stationarity of microbubbles. To cancel their motion, we have repeated the experiment. But a high number of repetition and a high value of iterations number could destroy the microbubbles and thus the energy could decrease. A trade-off must be found to avoid the destruction of the microbubbles.

These optimization could optimize the harmonic frequency of the microbubbles with our couple of transducers. The reception transducer has a bandwidth which corresponds with this frequency.

5. Conclusions

The optimization allows to have a not-inconsiderable gain for energy of backscattering signal. These methods allow to find the optimal frequency adapted to microbubbles.

We can carry on with complicating the optimization, first of all, with finding the optimal

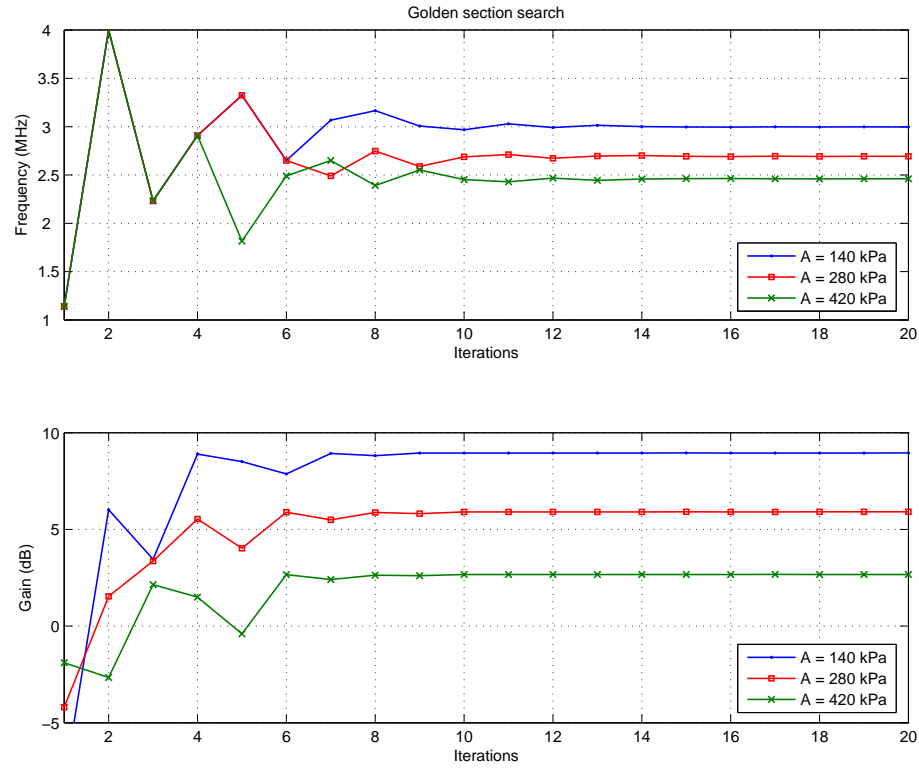


Figure 6. golden section search for a microbubble of 2 μm radius

frequency and the optimal amplitude simultaneously. Then we will try to distort a sinus curve in order to be close to the form described by Szeri [6].

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REFERENCES

1. W. H. Press, B. P. Flannery, S. A. Teukolsky, W. T. Vetterling, Numerical Recipes in Fortran, 2nd Edition, Cambridge University Press, 1992.
2. F. Michaut, Méthodes adaptatives pour le signal, Hermes, Paris, 1992.
3. C. Greis, Technology overview: SonoVue (Bracco, Milan), Eur Radiol Suppl 14 (8) (2004) 11–15.
4. Ir. S.M. van der Meer, Dr. M. Versluis, Prof.Dr. D. Lohse, C.T. Chin, A. Bouakaz, Prof.Dr. N. de Jong, The resonance frequency of SonoVue (tm) as observed by high-

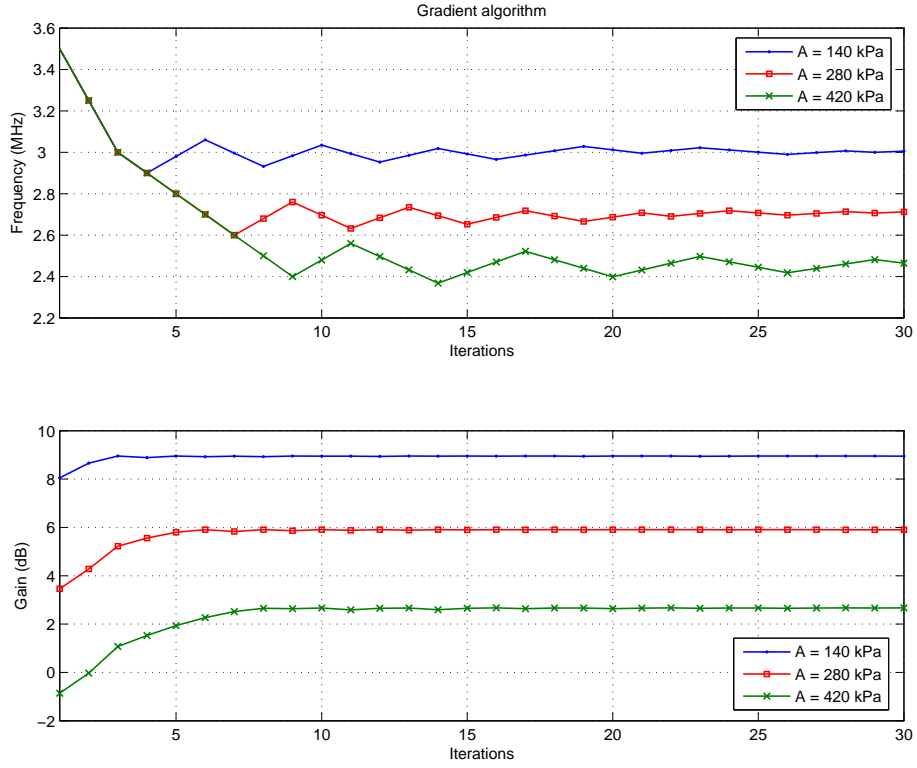


Figure 7. Gradient ascent for a microbubble of 2 μm radius

speed optical imaging, in: IEEE Ultrasonics Symposium, 2004, Vol. 1, IEEE, 2004, pp. 343–345.

5. L. Hoff, Acoustic Characterization of Contrast Agents for Medical Ultrasound Imaging, Kluwer Academic, Boston, 2001.
6. A. Reddy, A. Szeri, Optimal pulse-inversion imaging for microsphere contrast agents, Ultrasound in Med. & Biol. 24 (4) (2002) 483–494.

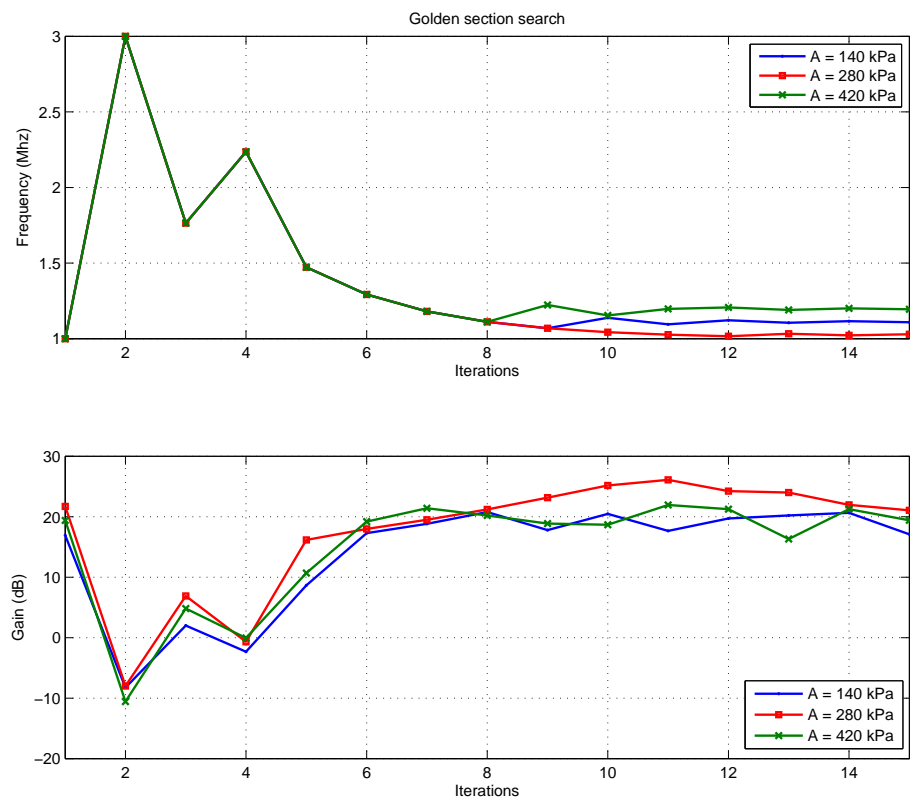


Figure 8. Experiment with golden section search

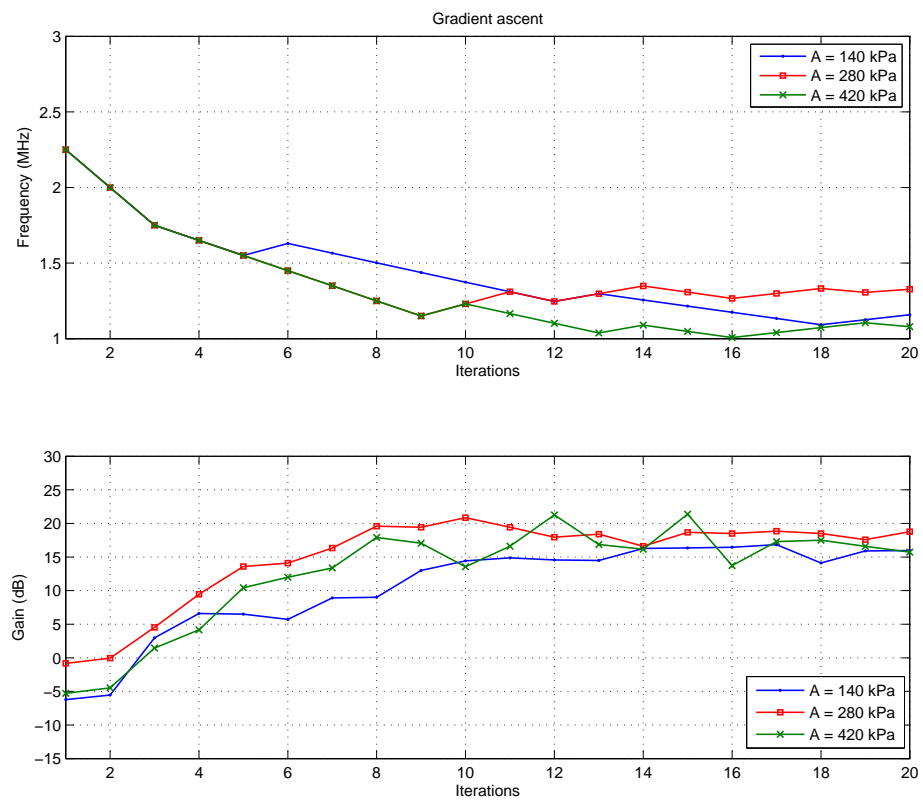


Figure 9. Experiment with gradient ascent